

## A Novel Percutaneous Device Realized the Prevention of Germ Infraction Made of a Nano-Scaled Hydroxyapatite Crystals/Polymer Composite

Kogai, Y<sup>1,2</sup>, Yasuda, S<sup>1,2</sup>, Okada, M<sup>2</sup>, Tanaka, J<sup>1,3</sup>, Furuzono, T<sup>1,2</sup>.

<sup>1</sup>Innovation Plaza Osaka, Japan Science and Technology Agency, Osaka, Japan.

<sup>2</sup>Department of Biomedical Engineering, National Cardiovascular Center Research Institute, Osaka, Japan.

<sup>3</sup>Independent Administrative Institution National Institute for Materials Science, Ibaraki, Japan.

**Statement of Purpose:** Various percutaneous devices, such as catheters for intravenous hyperalimentation (IVH), have been used in medical fields. However, there has been a serious problem regarding infectious agents entering from the outside through the gap between the skin and the device. To prevent the infection, various materials such as silicone, polyester, collagen, polyurethane, alumina, titanium, tantalum, and hydroxyapatite (HAp) have been applied to percutaneous devices since 1950 but sufficiently good results have not been clinically obtained.

We have been developed a novel inorganic/organic composite aiming at producing a percutaneous device which shows adhesiveness between soft tissue and the composite [1]. Attention in the development of the composite has been placed on the excellent bioactivity of HAp for hard or soft tissues. In this study, a prototype of percutaneous device was made of an inorganic/organic composite consisting of nano-scaled HAp crystals and silk fibroin (SF) via covalent bonding.

**Methods:** Nano-scaled HAp crystals were prepared by an alternating emulsion system, sintered at 800°C for 1 h [2]. The size of the HAp crystal was an a-axis length of 87±23 nm, a c-axis length of 236±81 nm, and a mean aspect ratio (c/a) of 2.72. Degummed fibers with 27-denier or *habutae* fabric made of silk from *Bombyx mori* were used as polymer substrates. Graft polymerization of  $\gamma$ -methacryloxypropyl trimethoxy-silane (MPTS) on the SF was conducted by free radical initiation. After the HAp crystals were suspended in a toluene/methanol (9/1, v/v) mixture solvent, the poly(MPTS)-grafted SF was soaked in the suspension. The SF adsorbed with HAp was heated at 120°C for 2 h in vacuum at 1 mmHg for a reaction between the HAp surfaces and the alkoxy-silyl groups of the poly(MPTS) grafted on SF to donate covalent bonding. A button-form substrate was made from a silicone compound by molding. HAp/SF fibers of about 100  $\mu$ m in length were thoroughly coated on the button. To detect initial cell adhesiveness on the samples, morphologies of fibroblast cells were observed with a scanning electron microscope (SEM).

**Results / Discussion:** The weight gain of poly(MPTS) on SF increased with increasing the reaction time, eventually reached a plateau value of about 15 wt%. Fig. 1 shows a SEM photograph of the HAp/SF composite fiber. The amount of the HAp bonded on the SF fiber was 13.1 wt%, which was 5 times larger than that on the SF fabric (2.8 wt%) under the same conditions. This means that it is hard for the HAp crystals to penetrate into the gaps between fibers in the fabric. The HAp crystals were bonded as aggregates, which is because a HAp crystal

consists of an a-plane with a cationic charge and a c-plane with an anionic charge.

To fabricate a prototype of a percutaneous device, the HAp/SF composite fibers were transplanted onto a button-form substrate made from a silicone via an adhesive agent. The HAp/SF composite fibers of 100  $\mu$ m in length could be transplanted uniformly and individually in random directions on the button (Fig 1). To evaluate the cell adhesiveness on the HAp/SF composite, the morphologies of L929 fibroblast cells incubated on the sample fabric or devices were observed by SEM. It is clear that cells favorably adhere only on the HAp surface of the composite but not on the dehydrated graft-surface without HAp crystals on the SF substrate. It is estimated that cell-adhesion proteins in serum, such as fibronectin, vitronectin, bFGF, etc., adsorb on the HAp surface much better than on the dehydrated graft-poly(MTPS).

**Conclusions:** Nano-scale HAp crystals were covalently bonded to the surface of the SF substrate through poly(MTPS) grafting on the substrate. The HAp coating was effective for improving the adhesiveness of the fibroblast cells. A button-form percutaneous device was fabricated by transplanting the HAp/SF composite fibers of about 100  $\mu$ m in length onto the surface of a button made from a silicone compound via an adhesive. The device was white and had good flexibility. Cells were able to penetrate into the space among the composite fibers in three-dimensional tangle. Soft tissue is expected to behave in a manner similar to the penetration of the cells into the device. Animal experiments with a percutaneous implantation of the button-form device for short to long period will be reported in this conference.

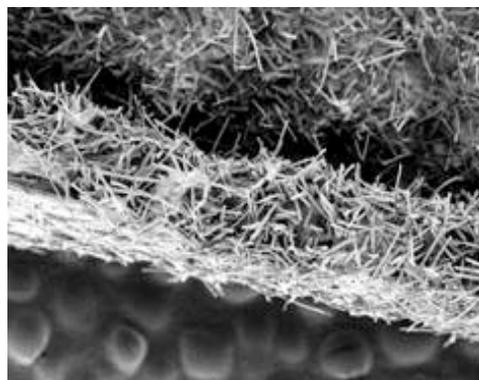


Fig. 1 A SEM photograph of the HAp/SF composite fibers on the prototype of a percutaneous device

**References:** [1] T. Furuzono, S. *et al.*, *J Artif Organs*, 2004;7: 137-144. [2] T. Furuzono *et al.*, *J Mater Sci Lett*, 2001;20: 1205-1212.