

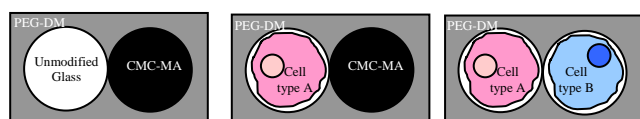
## Selectively Degradable Hydrogels for Investigating Cell-Cell Interactions in Co-culture

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**Statement of Purpose:** Interactions between neighboring cells regulate cell behavior as well as tissue function. Tools to investigate heterologous cell-cell interactions *in vitro* are therefore critically important for the development of new diagnostic and drug screening tools. A number of methods are available to study interactions between cells on patterned substrates [1]. Among these techniques, microfabrication and stereolithography provide powerful means to pattern cells [2], but typically rely on immobilized adhesive domains that permit stronger affinity of one cell type for a specific biochemical group relative to a second cell type. While successful, these techniques generally cannot be applied to co-cultures of similar cell types (e.g., two types of neurons) that do not demonstrate selective adhesion to biochemical cues. In this work, we aim to demonstrate a new co-culture patterning approach based on the selective degradation of patterned gels thus allowing the culture of *any* two cell types for investigating cell-cell interactions *in vitro*. Using maskless projection micro-stereolithography ( $\mu$ SL), we developed defined multi-component micropatterned architectures of poly (ethylene glycol) dimethacrylate (PEG-DM) and carboxymethyl-cellulose-aminoethyl methacrylate (CMC-MA) on glass substrates (Fig 1). Since both polymer surfaces are resistant to cell and protein adsorption [2,3], the first cell type can only adhere to the free glass spaces. The degradation of the CMC-MA patterns by the enzyme cellulase provides new adhesive regions on the substrate where a second cell type can adhere. This technique allows control of cell-cell contact and spacing between two different cell types at the microscale and will be used as a new tool to investigate heterologous cell-cell interactions in co-culture systems.

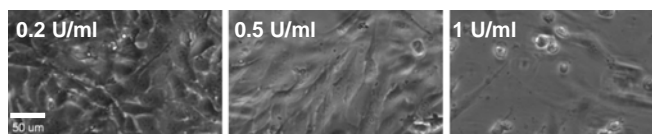
**Methods:** PEG-DM and CMC-MA were synthesized in house [3]. Viability of NIH 3T3 fibroblasts were tested in solutions of 0.2-1.0 U/ml cellulase (Sigma) and analyzed from phase microscopy (Olympus) images captured at 48 h. CMC-MA gel degradation in 0.2-1.0 U/ml cellulase solutions were verified by measuring the weight loss of 50  $\mu$ l CMC-MA gels and calculating degradation rate from the initial slope of gel weight loss versus time plots. To pattern the gels, a  $\mu$ SL system based on a digital micro-mirror device (DMD<sup>TM</sup>, Texas Instruments) was used to create the patterns. Gel precursor solutions were formulated by dissolving PEG-DM (60-80% w/v, 700 kDa) or CMC-MA (8-12%, 90 kDa) in 0.05% photoinitiator solution (Irgacure 2959, Ciba) prepared in phosphate buffered saline. Glass coverslips were modified with trimethoxypropylsilane-methacrylate (Sigma) to allow covalent linkage of the gels to the coverslip. The gels were crosslinked under UV light and the patterns are formed in a layer-by-layer fashion by modulating the UV light according to a defined mask on the DMD chip [4]. NIH 3T3 fibroblasts were seeded in the patterned coverslips in serum-containing media and incubated for 24 h. The



**Fig 1.** Schematic of approach. Step 1: PEG-DM and CMC-MA are patterned onto glass. Step 2: Cell type A is seeded onto the glass in serum-containing medium. Step 3: The CMC-MA pattern is degraded with cellulase and cell type B is seeded in serum-containing medium onto the newly exposed glass.

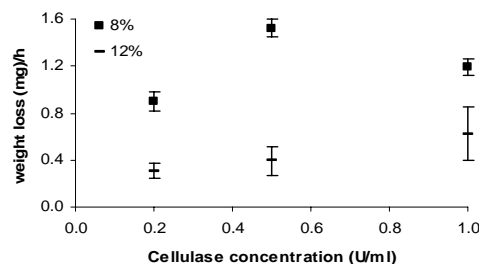
cell media was then replaced by fresh media containing cellulase every 1-2 h. Once the CMC-MA patterns were degraded, human SH-SY5Y neuroblastoma cells were added to the substrates and cultured in the same serum-containing media for 24 h. Images of the patterned substrates and selectively adhered cells were captured under phase microscopy.

**Results:** Preliminary viability studies (Fig 2) revealed that the fibroblasts were sensitive to cellulase only at high concentrations: when exposed to 0.2 or 0.5 U/ml cellulase for 48 h, the fibroblasts grew to confluence, whereas at 1 U/ml the fibroblasts had low viability.



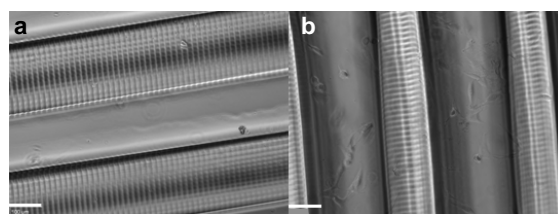
**Fig 2.** Phase contrast images of 3T3 fibroblasts cultured for 48 h in medium containing cellulase at 0.2-1.0 U/ml. (Scale bar, 50  $\mu$ m)

Degradation studies (Fig 3) indicate that gel degradation rates generally increase with greater cellulase concentrations and 8% CMC-MA gels degrade faster than 12% gels.



**Fig 3.** Degradation rates of 8 and 12% CMC-MA gels in 0.2-1.0 U/ml cellulase.

The  $\mu$ SL method was used to create polymer scaffolds of a variety of shapes and dimensions. Fig 4 depicts  $\sim$ 100  $\mu$ m PEG-DM channels (250  $\mu$ m Z-thickness) alone (a) and with co-cultured cells (b).



**Fig 4.** Phase contrast images of (a) micropatterned PEG-DM channels and (b) co-culture containing micropatterned substrates. Scale bar, 100  $\mu$ m.

**Conclusions:** The goal of this work was to demonstrate selectively degradable gels as a new tool for investigating cell-cell interactions in co-cultures. Preliminary studies demonstrate that cells can be seeded in the presence of cellulase, CMC-MA patterns can be effectively degraded and co-cultures can be maintained in the presence of  $\mu$ SL-micropatterned PEG-DM gels. Ongoing work focuses on optimizing co-culture patterning using the selectively degradable architectures. Immunohistochemical staining for fibroblasts and neuroblastoma cells will be used to verify the co-culture patterning.

### References:

1. Bhatia SN et al. JBMR 1997;34:189; Tsuda Y et al. BBRC 2006;348:937-44; Kidambi S et al. Macromol Biosci 2007;7:344-53; Hui EE et al. Langmuir 2007;23:4103-7.
2. Bhatia SN and Chen CS. Biomedical Microdevices 1999;2:131-44.
3. Reeves R, J Leach et al. in preparation.
4. Lu Y et al. JBMR 2006;77:396-405.