Synthesis and Characterization of Chondroitin Sulfate Methacrylamide Micelles

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Introduction: Micelles are stable, self-assembling particles that are capable of delivering drugs and growth factors in an aqueous environment. Chondroitin sulfate (CS) is a common glycosaminoglycan found in tissues such as cartilage and is highly negatively charged. Amphiphilic CS-poly(L-lactic acid) and CS-poly(lacticco-glycolic acid) microspheres have been previously reported for use as drug delivery carriers (Lee CT. Biomacromolecules. 2006;7:1179-86. Lee ES Biomaterials. 2007;28:2754-62). The negatively charged nature of CS makes it an appropriate material for polyionic complexation with cationic molecules, including growth factors such as basic fibroblast growth factor and transforming growth factor β 1. In these studies, we describe the synthesis and characterization of novel chondroitin sulfate methacrylamide (CSMAm) micelles for tissue engineering and bioactive factor delivery.

Methods: N-(3-aminoproyl) methacrylamide (Polysciences, Warrington, PA) was covalently conjugated to chondroitin sulfate A (Sigma Aldrich, St. Louis, MO) using N-(3-dimethylaminopropyl)-N'ethylcarbodiimide (Sigma Aldrich) chemistry in distilled water. The reaction mixture was dialyzed for a total of 72 hrs (1,000 Da molecular weight cutoff), and the product was lyophilized for 4 days.

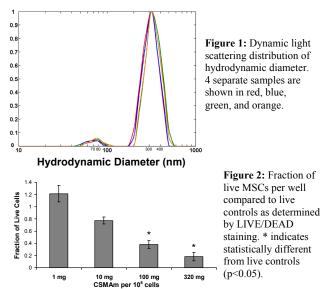
CSMAm micelle formation in distilled water was verified using light microscopy and dynamic light scattering (DLS). A solution of CSMAm in distilled, deionized water (ddH₂O) was mixed with 1 µm diameter latex microspheres (Polysciences), and particles were observed under light microscopy at a total magnification of 100X to determine the morphology and relative size of CSMAm micelles. DLS measurements were taken to determine the hydrodynamic diameter of CSMAm micelles in ddH₂O, and zeta potential measurements were also recorded as a measure of surface charge and colloidal stability. DLS (n=4) and zeta potential (n=3)measurements were recorded at 23°C in ddH₂O (Particle Sizing Systems NICOMP 380ZLS, Santa Barbara, CA), while samples of unmodified CS at the same concentration served as controls.

Cytotoxicity was characterized *in vitro* using bovine marrow stromal cells (MSCs). MSCs were plated at 10,000 cells/cm² in a tissue culture-treated 96-well plate, and cultured in media containing CSMAm equivalent to 1, 10, 100, 320 mg per 10^6 cells. After 24 hrs of exposure, cells were stained with LIVE/DEAD solution (Invitrogen, Carlsbad, CA), causing live and dead cells to fluoresce green and red, respectively. Fluorescence was measured in a plate reader (n=3), and relative viability was analyzed in comparison to live controls. Statistical significance was determined using a one-way ANOVA with Tukey's multiple comparison test (p<0.05).

Results: Light microscopy images indicate that CSMAm micelles were smaller than 1 μ m diameter microspheres,

providing a qualitative estimation of the relative size. DLS measurements indicated that a bimodal distribution of the CSMAm micelles were formed, with average diameters of 324.1 ± 8.5 nm and 73.2 ± 4.4 nm (Figure 1). Unmodified CS, however, did not produce sufficient levels of scattering for DLS measurements. Zeta potential measurements showed that the micelles possessed a zeta potential of -38.7 ± 1.1 mV, indicating that CSMAm micelles were negatively charged and stable in solution.

LIVE/DEAD staining of bovine MSCs in the presence of increasing concentrations of CSMAm revealed that cells remained largely viable at the lowest concentrations of 1 and 10 mg/10⁶ cells with 1.21 ± 0.14 and 0.77 ± 0.05 viability, respectively, compared to live controls (Figure 2). A significant decrease in viability was observed at 100 mg and 320 mg/10⁶ cells concentrations with 0.38 ± 0.06 and 0.18 ± 0.07 viability, respectively.



Conclusions: These results confirm that CS-based nanoparticles were formed via modification of CS with methacrylamide. These highly negatively-charged CSMAm micelles may have application in delivery and controlled release of cationic growth factors by pH-driven dissociation or enzymatic cleavage by chondroitinase. The presence of CS itself may also directly influence cell behavior, including proliferation, ECM production, and differentiation (van Susante JLC. Biomaterials. 2001;22:2359-69. Varghese S. Matrix Biol. 2008;27:12-21. Wu YN. Biomaterials. 2007;28:4056-67). The concurrent delivery of CS matrix molecules and soluble factors may simultaneously affect cell function, making this an exciting technology for bioactive factor delivery for a variety of regenerative medicine applications.

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