

## Elucidating Endothelial Cell Hemostatic Regulation by Isolating Integrin-mediated Adhesion to Bioactive Hydrogels

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**Statement of Purpose:** A major limitation of early blood-contacting medical devices was their propensity to fail due to thrombosis. Significant research effort has been made to develop antithrombotic coatings for blood-contacting devices to address this limitation. The native cardiovascular system produces anti-thrombotic surfaces through the utilization of an endothelial cell (EC) monolayer covering all blood-contacting surfaces in the body. The EC monolayer prevents platelet activation, provides a protective and selective barrier to underlying tissues, responds to injury, and activates clotting when necessary by releasing pro- and anti-thrombotic factors. Studies have demonstrated that EC phenotype and expression of hemostatic regulators is dependent on the ECM substrate, suggesting that integrin and syndecan binding affects regulation of hemostasis. However, the individual and synergistic roles of integrin binding on intracellular signaling leading to different expression of pro- and anti-thrombotic factors is not well understood. We hypothesize that elucidation of integrin-mediated hemostatic function of ECs will allow for the design of biomaterials with sustained thromboresistance. In this study, we present the first phase of isolating specific EC integrin interactions using a combination of ECM surfaces and antibody blocking. These systems will then be used to examine EC hemostatic function and finally design materials with targeted integrin interactions as thromboresistant coatings for blood contacting devices.

**Methods:** *Protein hydrogels:* To generate bioactive hydrogels with different ECM components, rat tail collagen I and bovine gelatin type B were first functionalized with acrylate-PEG-N-hydroxysuccinimide (Acr-PEG-NHS) at a ratio of 0.1:1 of the protein lysines. Functionalization was confirmed with FTIR spectroscopy. Functionalized protein was then added at 4 mg/ml to a hydrogel precursor solution (poly(ethylene glycol) diacrylate (PEGDA), 10%) and crosslinked under UV light with 1% Irgacure. *Integrin expression with flow cytometry:* HUVECs cultured in tissue-culture treated poly(styrene) T-75 flasks to 90% confluence and released from flasks using TrypLE Express 1:10 in sterile PBS. Cells were spun down and resuspended in flow buffer (PBS with 2% FBS) at a concentration of  $10^6$  cells/mL with 1 mL samples. Cells were then stained with fixable viability dye 450 for 20 minutes on ice then washed with 3 mL flow buffer. Cells were then incubated with the respective integrin antibody (anti- $\alpha 1$  and anti- $\alpha 2$  at 5  $\mu$ L/mL; anti- $\alpha V$  and anti- $\alpha 5$  at 2.5  $\mu$ L/mL) on ice for 30 minutes. Cells were again washed with flow buffer and resuspended in 400  $\mu$ L 4% paraformaldehyde to fix the cells. Surface expression was then analyzed using the BD LSR II Flow Cytometer. Relative fluorescence was used to compare levels of expression. *Integrin-specific adhesion:* Antibodies for integrins were added to HUVECs and allowed to incubate at room temperature for 15 min before adding cells to the substrates and incubating at 37°C for 30 min: anti-

integrin  $\alpha 1$  (13.3  $\mu$ g/mL); anti-integrin  $\alpha 2$  (6.65  $\mu$ g/mL); anti-integrin  $\alpha V$  (2.5  $\mu$ g/mL); anti-integrin  $\alpha 5$  (3.33  $\mu$ g/mL); anti-integrin  $\beta 1$  (3.33  $\mu$ g/mL). Samples were washed 2X with PBS then fixed with 3.7% glutaraldehyde and stained with rhodamine phalloidin and SYBR green for imaging.

**Results:** HUVEC integrin expression with flow cytometry indicated that  $\alpha 2\beta 1$  was the most highly expressed and integrins  $\alpha 5\beta 1$  and  $\alpha V\beta 3$  were both expressed at levels approximately 50% compared to  $\alpha 2\beta 1$ . The expression of integrin  $\alpha 1\beta 1$  was only about 20% compared to  $\alpha 2\beta 1$  and antibody blocking of  $\alpha 1$  displayed little difference in HUVEC attachment on collagen hydrogel compared to the non-blocked control. Similarly, there was little reduction in attachment when blocking  $\alpha V$ , as expected as there are no available binding sites for  $\alpha V\beta 3$  or  $\alpha 5\beta 1$  integrins on collagen. In contrast, a significant reduction in attachment was observed when blocking  $\alpha 2$ . These findings indicate that  $\alpha 2\beta 1$  was the primary integrin involved in HUVEC attachment to the collagen hydrogel. Of note, a further reduction was observed by combining  $\alpha 1$  and  $\alpha 2$  integrin blocking, suggesting that there is some compensatory mechanism of  $\alpha 1\beta 1$  interactions when  $\alpha 2\beta 1$  is unavailable. On gelatin hydrogels, blocking  $\alpha 2$  resulted in very little difference in HUVEC attachment as expected given the loss of  $\alpha 2\beta 1$  affinity with loss of triple helix conformation. Significant reduction in attachment was observed when blocking  $\alpha V$  and  $\alpha 5$  with a further reduction observed by combining  $\alpha V$  and  $\alpha 5$  blocking. This indicates that integrins  $\alpha V\beta 3$  and  $\alpha 5\beta 1$  contribute somewhat equally to HUVEC attachment to gelatin, and each interaction can be isolated with selective antibody blocking.

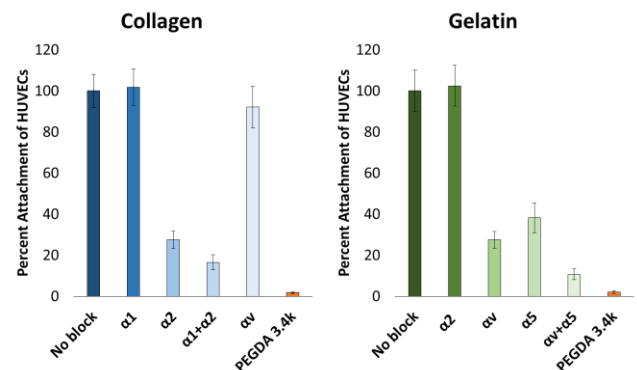


Figure 1: Attachment of HUVECs on protein hydrogels with integrin blocking using integrin antibodies.

**Conclusions:** We have demonstrated a method to isolate individual integrin interactions of HUVECs on ECM hydrogels. This will allow us to then correlate changes in hemostatic regulator protein gene expression, specifically TF, TFPI, ADAMTS-13, VWF, tPA, eNOS, and PAI-1, to specific integrin-mediated attachment and elucidate individual and synergistic effects. Integrin-targeting proteins can then be utilized in hydrogel coatings to promote not only EC attachment and migration, but also a thromboresistant phenotype.